

"Dunarea de Jos" University of Galati Faculty of Metallurgy and Material Science



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	Ovidiu DIMA - PERMANENT FORMS FOR CASTING MORE SUSTAINABLE,	
==	CLADDING HARD ALLOYS.	264
15	CLADDING HARD ALLOYS	
		272
		212
*		
		280
		200
5		
		284
	FLEXURAL STRENGTH OF TWO CERAMIC SYSTEMS PERJU. Mihai AXINTE -	
=	Ion HOPULELE, Carmen NEJNERU, Manuela Cristina PERJU, Mihai AXINTE -	290
	THIN LAYERS OBTAINING BY ELECTRIC SPARK IN LIQUID MEDIUM	*
35	V.G. GRECHANYUC, N.I. GRECHANYUC, Lucica ORAC - CORROSION	
	V.G. GRECHANYUC, N.I. GRECHANYUC, Edita ONICE RESISTANCE IN NEUTRAL SALINE FOG OF THE COMPOSITES Cu-Mo OBTAINED	297
	BY PVD METHOD SOW POLITION WITH HEAVY METALS	305
5	Maria VLAD, Gelu MOVILEANU - SOIL FOLD Marian BORDEL - CONSIDERATION	
5	Alexandru STANCIOIU, Olga MITOSERIU, Marian BORDEN REGARDING THE HEAT TREATMENT OF SHEETS AND STRIPS FROM	
	REGARDING THE HEAT TREATMENT OF SHEET	309
	ALUMINUM ALLOY 5052 TYPE	
=	ALUMINUM ALLOY 5052 TYPE	
	THEORETICAL STUDY REGARDING THE 120	313
		221
5	OF CYLYNDRICAL CASTED PARTS WITH SMALL THICKNESS	321
	OF CYLYNDRICAL CASTED PARTS WITH SMALL THICKNESS Tamara RADU, Lucica BALINT, Viorel DRĂGAN – RESEARCH ON THE EFFECT OF Tamara RADU, Lucica BALINT, VIORE DAMERSION ON THE LAYER THICKNESS	
54	Tamara RADU, Lucica BALINT, Viorel DRAGAN - RESEARCH OF THE LAYER THICKNESS TEMPERATURE AND DURATION OF IMMERSION ON THE LAYER THICKNESS TEMPERATURE AND DURATION OF IMMERSION ON THE LAYER THICKNESS	226
	OF ZINC COATING OBTAINED IN MICROALLOYED ZINC MELTS	326
==	OF ZINC COATING OBTAINED IN MICROALLOTED ZINC INDICATING CARBIDE Stela CONSTANTINESCU – CHARACTERISATION OF NIOBIUM CARBIDE STELA CONSTANTINESCU – CHARACTERISATION OF NIOBIUM CARBIDE STELA CONSTANTINESCU – CHARACTERISATION OF NIOBIUM CARBIDE	331
-	CHEMICAL DEPOSITION FROM VAPOUR AT NORMAL PRESSURE	331
50	CHEMICAL DEPOSITION FROM VAPOUR AT NORMAL TRANSPORTER, Nartzislav Dimitar TEODOSIEV, Lubomir ANESTIEV, Jordan GEORGIEV, Nartzislav Dimitar TEODOSIEV, Cristiana NIKOLOVA – GLASS- CARBON	
-	Dimitar TEODOSIEV, Lubomir ANESTIEV, Jordan GEORGIA, PETROV, Petar TZVETKOV, Cristiana NIKOLOVA - GLASS- CARBON	338
	PETROV, Petar TZVETKOV, Cristiana (MROSOV) BIOACTIVE COATINGS ON A TiO2- Nb2O5 SUBSTRATE	550
-	BIOACTIVE COATINGS ON A TIO2- NO2O5 SUBSTRATE PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Ioan SARACIN, Olimpia PANDA - Alexandru CHIRIAC, Gheorghe FLOREA, Gheorghe FLORE	346
	Alexandru CHIRIAC, Gheorghe FLOREA, 10an SARACHA, SARACHA	
58	SOURCES OF EMISSIONS IN THE SINTERING AND BEAST TOWN OF LOSAN - INFLUENCE OF LOSAN CIOBANU, Diana TUTUIANU, Tibor BEDŐ, Aurel CRIŞAN - INFLUENCE OF	351
	RIB LENGHT ON THE SOLIDIFICATION OF CAST PARTS	
5	Ioan CIOBANU, Diana TUTUIANU, TIDI DEOC CAST DARTS	360
	RIB THICKNESS ON THE SOLIDIFICATION OF CAST PARTS Violeta VASILACHE, Sonia GUTT, Ion SANDU, Gheorghe GUTT, Traian	
5		
	VASILACHE - ELECTRODEPOSITION AND CHARGET	370
	ZINC-COBALT ALLOY COATINGS NEW DISTALLATION OF ELABORATION-	
1	Vasile BAŞLIU – DEVELOPMENT OF A NEW INSTALLATION OF DEVELOPMENT OF A NEW INSTALLATION OF CASTING IN ORDER TO OBTAIN COMPOSITE MATERIALS WITH METALLIC	
	CASTING IN ORDER TO OBTAIN COMINGSTIE MATERIAL	375
	MATRIX	1 400
1	Alexandru CHIRIAC, Gheorghe Florea, Marian NEACSO, Ioan State BRASS PANDA - STRUCTURAL ASPECTS OF ANTIFRICTION PROPERTIES BRASS	380
	PANDA - STRUCTURAL ASPECTS OF ASIA WOR OF SOME NON-CONVENTIONAL	
7	TREATED STEELS DURING WEAR PROCESS (III)	386
	TREATED STEELS DUKING WEAK PROCESS (III)	

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MATERIALS FOR TOTAL HIP JOINT PROSTHESES: BIAXIAL FLEXURAL STRENGTH OF TWO CERAMIC SYSTEMS

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ABSTRACT

Total hip joint replacement is one of the most successful orthopaedic surgeries in the last decade. Essential part of total hip joint prostheses is the mobile joint "hemispherical head - hemispherical cup". Functional properties and durability of the implanted prosthesis in the human body depends crucially on the mechanical and tribological properties and characteristics of materials of articulated parts.

Development and improvement of implant technology is inextricably linked with the development of new materials and, in particular, new ceramic materials with improved mechanical characteristics. This in turn requires improving methods of preliminary testing and evaluation of these characteristics.

In the paper materials for hip prostheses and methods for evaluation of their mechanical characteristics are briefly reviewed. The results of preliminary studies on some characteristics of reinforced titanium ceramics are presented.

KEYWORDS: bioceramics, flexural strength

1. Introduction

Along with high biocompatibility and durability of materials used for hip replacement are their mechanical properties. There are a number of standardized procedures for determination of suitability of different materials.

For making different types of prostheses are used as metal (steel and titanium) alloys and various types of ceramics. Two types of ceramic materials are used in practice - type A and type B. Type A ceramic materials for implants are subjected to high loads (bearing surfaces of joint implants), and type B are intended for use in implants with small loads (implants for middle ear).

Fundamental mechanical tests for ceramic materials for arthroplasty under ISO 6474:1994 (E) relating to the definition average biaxial flexure load and resistance of the material, such as durability at the material is examined in cases where the saticulation of ceramics on ceramics.

2. Biaxial flexure testing

When examining the biaxial flexure least [1], disk made of research material is placed between two coaxial rings of different diameters.

Gradually increasing compressive loads applied and its value at fracture of the specimen is registered. The Flexural Strength is calculated based on the results of the recorded fracture load (F).

The specimen, loading and supporting are shown schematically in Fig. 1 and Fig. 2a. Fig. 2b.



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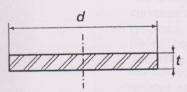


Fig.1. Shape and dimensions of the specimen

Principle scheme of measuring the strength of biaxial flexure is presented in Fig.3. Between the supporting ring (2) and the specimen (3) a rubber pad (8) is placed to exclude the influence of shape deviations of the contact surfaces of the specimen and the rings. The loading ring (4) transmits the load to the specimen through a thin paper pad (7). For Uniformly distribution of the load on the specimen, the load given by the loading device of the machine for testing tension/compression load (6) is transmitted through the metal sphere (5) to the loading ring (4)

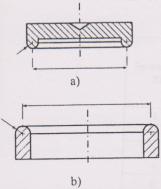


Fig. 2. Loading (a) and supporting (b) rings

The fracture load F of the specimen is registered. The flexural strength is given by:

$$\sigma = \frac{3F}{2\pi r^2} \left[(1 + v) \ln \left(\frac{d_s}{d_c} \right) + (1 - v) \left(\frac{d_s^2 - d_c^2}{2d^2} \right) \right]$$
 (1)

Where:

t – mean thickness, determined by 3 measuring of the specimen, mm;

d_s – average contact diameter of the supporting ring, mm;

d_e - average contact diameter of the loading ring, mm;

d - average diameter of the specimen, mm;

v - Poisson's ratio was taken as 0,25 for all ceramics according to the recommendation in the standard

The specimens are loaded in a universal testing machine INZTRON 1195. The loads applied to the surface of the specimen via loading ring at a rate of 540 N/s.

The diameters of the contact circles of the supporting and loading rings are de=12,01, mm and ds=30,14, mm, radius of the curvature of the contact surface with the specimen is r=2,01 mm. Rubber pad placed between the specimen and the supporting ring has a 0,6 mm thickness and scleroscope hardness 62. The contact surfaces of the rings are hardened to 42 HRC.

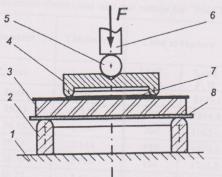


Fig.3 Loading Scheme
1-base; 2-supporting ring; 3-specimen;
4-loading ring; 5-contact sphere;
6-loading element; 7-paper pad;
8-rubber plate.

The diameters of the contact circles of the supporting and loading rings are de = 12,01

Mai 14 -15, 2010, Galap, România



mm and ds = 30,14 mm, radius of the curvature of the contact surface with the specimen is r=2,01 mm. Rubber pad placed between the specimen and the supporting ring has a 0,6 mm thickness and scleroscope hardness 62. The contact surfaces of the rings are hardened to 42 HRC.

2. Materials and results

Materials used in the paper are aluminium and reinforced titanium ceramics. The test specimens [3] are obtained by the same technology used for making hip-joints femoral heads.

Aluminium ceramic

Ten pieces of "MARTOXID" ceramic (99,5% Al2O3 and 0,3% MgO) [2] MartinSWERK, used for manufacturing hip-joint prosthesis, were subjected to flexural strength test.

The dimensions of the specimens diameter (d_m) and thickness (t_m), are given in Table 1. In the same table are given

values of the fracture load F and according to formula flexural strength

Reinforced titanium ceramir

The ceramic specimens tesser prepared by mixing TiO2 and Nb2O in proportions ensuring concentration wt.%. Nb2O5 in the final product preparation of the samples is described details in [Teodosiev and all Ances Control [4].

The as prepared specimens were at temperature of 1450°C (8 specimes) 1520° (8 specimens) according predetermined temperature regime.

The dimensions of the spectrum diameter (dm) and thickness (tm), are green Table 2 and 3 for type 1 and 2. In the tables are given values of the fracture load and flexural strength.

The tested specimens after fracture shown in Fig. 4, 5 and 6.

Table. 1. Specimens dimensions and test results for "MARTOXID" ceramic

Specimen No	Diameter Thickness d_m , mm t_m , mm	Thickness	Load at rapture		Biaxial flexure strength at rapture
		Load F, kg	Load F, N		
1	36,00	2,28	215	2109,2	-
2	35,83	2,126	185		265,6431
3	36,13	2,168	200	1814,9	263,2938
4	36,23	2,144		1962,0	272,9844
5	36,30	2,086	195	1913,0	271,9115
6	36,27		180	1765,8	264,9839
7	35,77	2,17	195	1913,0	265,3413
8	35,97	2,128	185	1814,9	262,9425
9		2,152	195	1913,0	270,5183
10	36,27	2,168	190	1863,9	
10	36,03	2,13	180	1765,8	259,0150
					254,7572
		-	σ; , MPa		265,1391
			s, M	Pa	5,678312



Mai 1+ 15, 2010, Galan, România



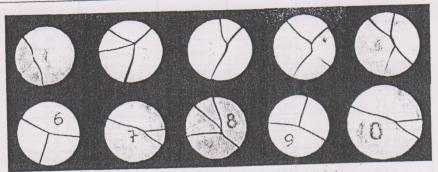


Fig. 4. Specimens from "MARTOXID" ceramic after fracture

Table.2 Specimens dimensions and test results for reinforce titanium ceramic - type 1

Specimen	Diameter		Biaxial flexure strength at rapture	
N2	d_m , mm t_m , mm	t _m , mm	Load F, N	σ, MPa
1-1	34.25	1.976	533	90.9
1 -2	34.08	2.042	494	79.0
1 -3	34.24	1.950	486	85.1
1-3	34.15	2.160	750	107.2
1 -5	34.3	2.080	673	103.5
1 -6	34.13	2.120	984	145.9
1 - 7	34.13	2.120	751	111.2
	34.2	2.124	733	108.2
1 -8	34.2	2.12	σ; , MPa	103.87
			s, MPa	19.33

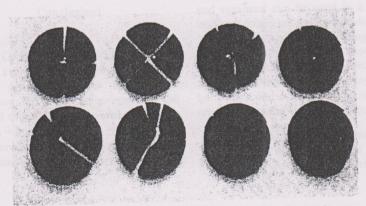


Fig. 5. Specimens from reinforced titanium ceramic - type 1 after fracture

the 5 th edition Mai 14 15, 2010, Galap, România



Table.3 Specimens dimensions and test results for reinforce titanium ceramic - type 2

Specimen	Diameter Thickness		Load at rapture	Biaxial flexure strength at rapture
№	d_m , mm	t _m , mm	Load F, N	σ, MPa
2-1	34.32	2.244	538	71.1
2-2	34.8	2.215	919	124.0
2-3	34.25	1.980	458	77.8
2-4	34.3	2.080	720	110.7
2-5	34.23	2.183	901	126.0
2-6	34.16	2.081	640	98.5
2-7	34.16	2.124	556	82.1
2-8	34.45	2.213	720	97.7
20			σ; , MPa	98.48
			s, MPa	19.37

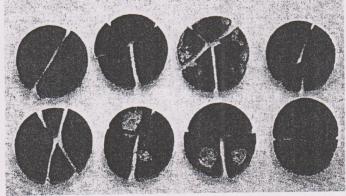


Fig.6. Specimens from reinforced titanium ceramic - type 2 after fracture

Conclusions

Studied samples of ceramics "MARTOXID", MartinSWERK, showed that the average flexural strength at biaxial flexure testing is σ ; = 265,1 MPa. According to the requirements of the standard the minimum flexural strength is σ ; min = 250 MPa.

Therefore the test samples meets the requirements of the regulations for type A

and ceramics can be used in a production to implants subjected to large loads.

The average flexural strength of titanium ceramic samples does not meet the requirements. For further investigation of this ceramics their manufacturing technology must be improved so they can meet the requirements for hip-joint prosthesis.

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the 5th edition Mai 14-13, Loss, Galan, România



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